

CRITCARE BITES

CARDIAC OUTPUT MONITORING

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M A D F O R M E D I C I N E

OVERVIEW

- Background
- Indication
- Monitoring methods
- Pulse contour analysis
- Transpulmonary thermodilution
- Pulmonary artery catheter
- Others

BACKGROUND

- Cardiac output monitoring devices derive cardiac output (in different ways) and other haemodynamic parameters
- Devices differ: Parameters, invasiveness, limitations
- Basic ICU haemodynamic monitoring: Arterial line, CVC, ultrasound
- Use cases: Cardiogenic/mixed shock, high doses of vasoactive medication, failure to respond to treatment
- Generally, less invasive modalities have not been shown to be accurate in critically ill patients

INDICATION/USES

- Assess fluid responsiveness: Change in stroke volume, stroke volume variation
- Etiology of shock: Cardiac index, systemic vascular resistance, preload indices
- Phenotyping in cardiogenic shock
- Guide/assess response to treatment
- Fluid status/tolerance: EVLWI, PAOP

MONITORING METHODS

Non-Invasive

- Bioimpedence/
Bioreactance
- Volume clamp/
radial artery
applanation
tonometry

Minimally Invasive

- **Arterial line
pulse contour
analysis**
- Esophageal doppler

Invasive

- **Transpulmonary
thermodilution**
- **Pulmonary
artery
catheterisation**

MEASUREMENTS

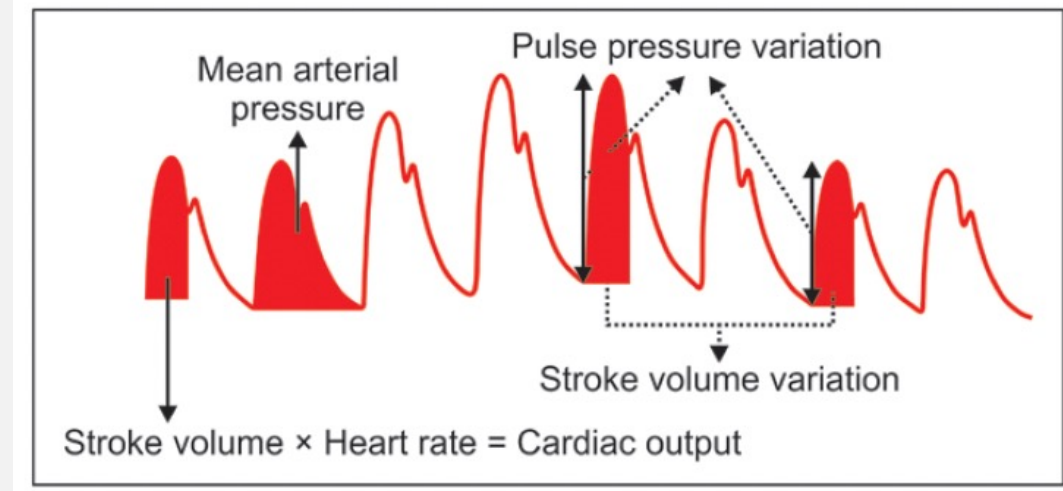
	Pulse Contour Analysis	Transpulmonary Thermodilution	Pulmonary Artery Catheter
Preload	-	Global end-diastolic volume	CVP (right), PCWP (left)
Contractility	-	Cardiac function index, global ejection fraction	PAPI (RV function) = $((\text{PAS} - \text{PAD}) / \text{RAP})$
Afterload	$\text{SVR} = [(MAP - CVP) / CO] \times 80$	SVR	SVR PVR = $[(mPAP - PCWP) / CO] \times 80$
Cardiac Output/Stroke Volume	SV CO (HR x SV)	CO	CO RVEF
Fluid Responsiveness	SVV	SVV (when paired with pulse contour analysis)	-
Fluid tolerance	-	Extra vascular lung water Pulmonary vascular permeability	-

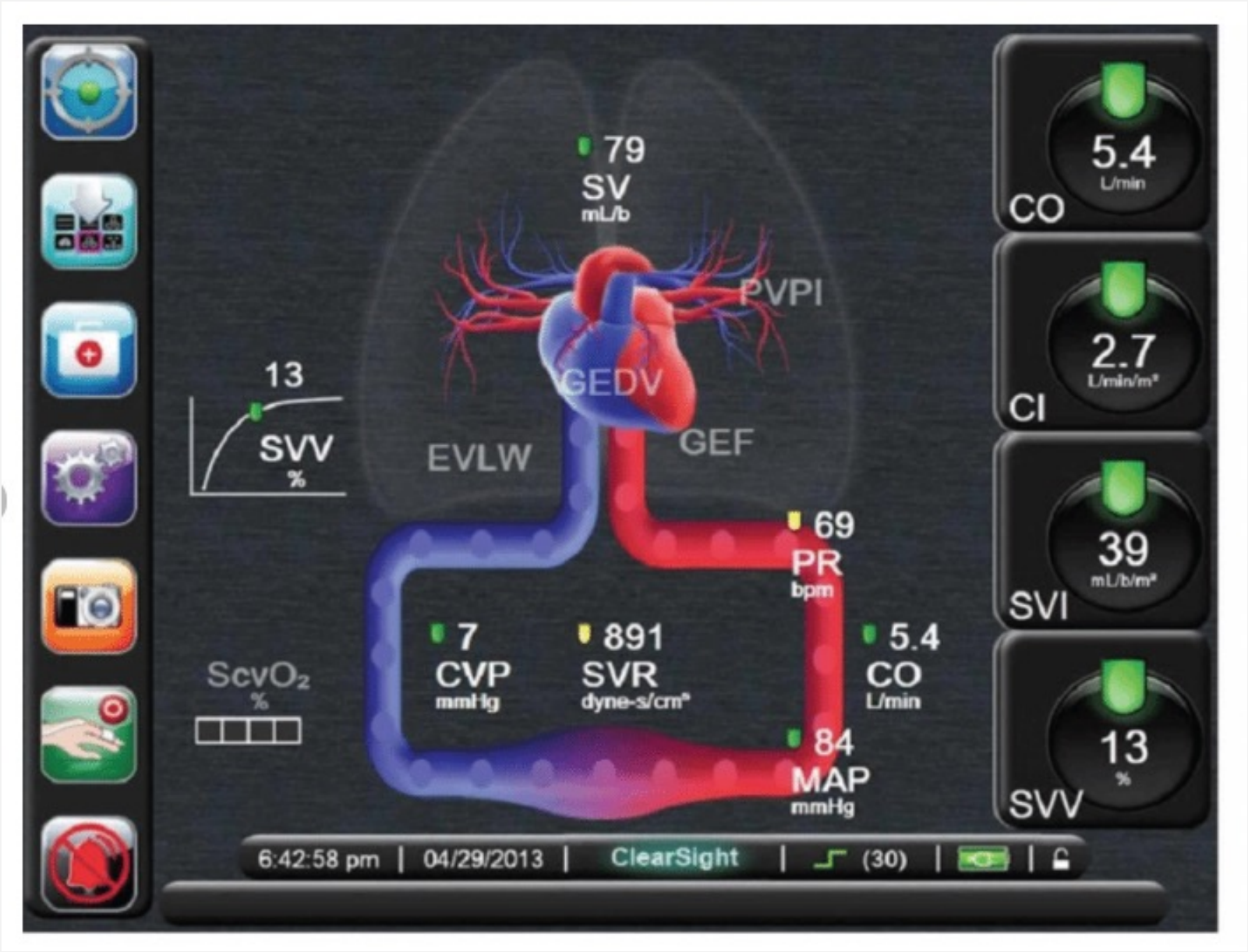
'NORMAL' VALUES

General	Transpulmonary Thermodilution	Pulmonary Artery Catheterisation
<ul style="list-style-type: none"> • CO: >5L/min • CI: >2.2 L/min/m² • SV: 50-100ml • SVI: > 35 ml/m² • SVR ((MAP – CVP) / CO) x 80): 800-1200 dynes s/cm⁵ • SVRI: 1700-2400 dynes s m²/cm⁵ 	<ul style="list-style-type: none"> • GEDVI: >700 • EVLWI: <10 • PVPI: <3 • CFI: >5 	<ul style="list-style-type: none"> • CVP < 14, PCWP <18 • mPAP < 25 • PAPI ((PAS-PAD)/RA) >1.5 • CPO (MAP x CO / 45 l): 0.5-0.7W/m² • RVEF: >35% • PVR ((mPAP-PCWP)/CO) x 80): 100-200 dynes/cm⁵ • PVRI: 250-300 dynes s m²/cm⁴

PULSE CONTOUR ANALYSIS

- **Arterial pulse pressure and its contour are analysed** and a **stroke volume is determined** from the **area under the systolic part** of the arterial curve, based on the principle of **ventriculo-arterial coupling**
- Pulse contour analysis can be externally calibrated (e.g. based on values derived from echocardiography or thermodilution) or internally calibrated (based on patient-specific anthropometric and demographic data to adjust for arterial compliance and tone)
- Application
 - Non-invasive: Volume clamp, radial artery applanation tonometry
 - Non-calibrated via IA line: E.g. Flotrac
 - Calibrated: Calibration with transpulmonary thermodilution (e.g. PiCCO, VolumeView)





	Pulse Contour Analysis
Preload	-
Contractility	-
Afterload	$SVR = [(MAP - CVP)/CO] \times 80$
Cardiac Output/Stroke Volume	SV CO (HR x SV)
Fluid Responsiveness	SVV
Fluid tolerance	-

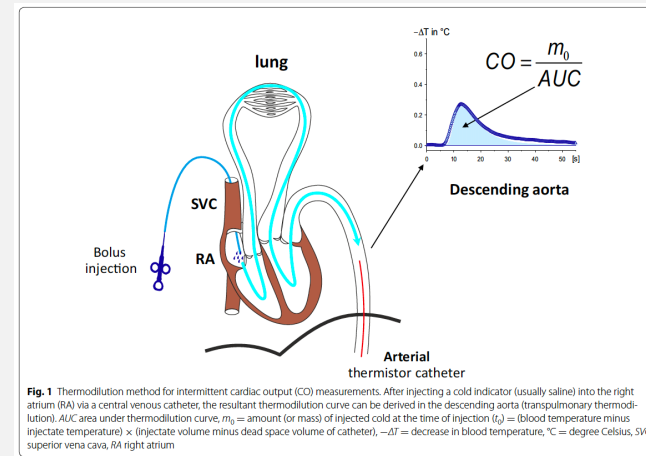
IVC Size	IVC Collapsibility	Interpretation (CVP)
< 1.5cm	>50% collapsibility	0-5 mm Hg (Low CVP)
< 1.5-2.5cm	>50% collapsibility	6-10 mm Hg
1.5-2.5cm	<50% collapsibility	11-15 mm Hg
>2.5cm	<50% collapsibility	16-20 mm Hg (High CVP)

PULSE CONTOUR ANALYSIS

- Advantages:
 - Automated
 - Continuous, beat-by-beat
 - User-independent measurement technique
- Disadvantages (uncalibrated devices):
 - Bias of proprietary algorithms (based off healthy population, hence unclear reliability in haemodynamically unstable patients with changing arterial resistance)
 - Subject to drift over time (without calibration)
 - Limited hemodynamic variables provided (CO, PPV, SVV)

TRANSPULMONARY THERMODILUTION

- Transpulmonary thermodilution technologies (e.g. PiCCO, VolumeView) offer haemodynamic insights through **thermodilution, pulse contour analysis and intrathoracic volumes**
- Cardiac output is determined by administration of a cold injectate via an internal jugular central line and detection of temperature change through a femoral arterial catheter. A **thermodilution curve allows for calculation of cardiac output using the Stewart-Hamilton equation** (cardiac output is inversely related to area under thermodilution curve)
- While thermodilution is intermittent, incorporation of calibrated **pulse contour analysis** allows for real-time monitoring of cardiac output

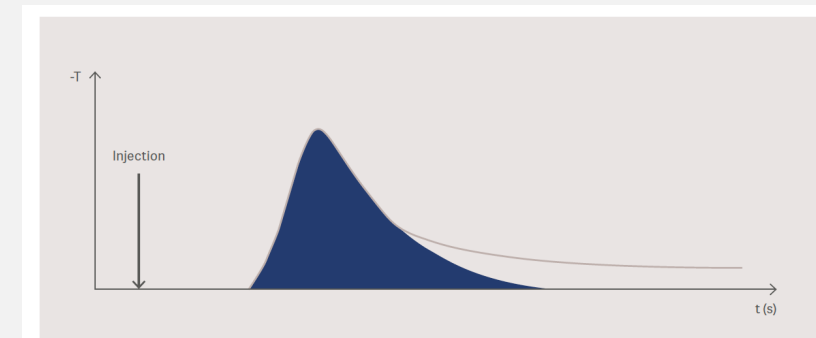


15ml of cold saline < 8 degC injected quickly, average across 3 readings

Blood temperature	Injectate temperature	Injectate volume	Correction constant*
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$$CO = \frac{(T_b - T_i) \times V_i \times K}{\int \Delta T_b \times dt}$$

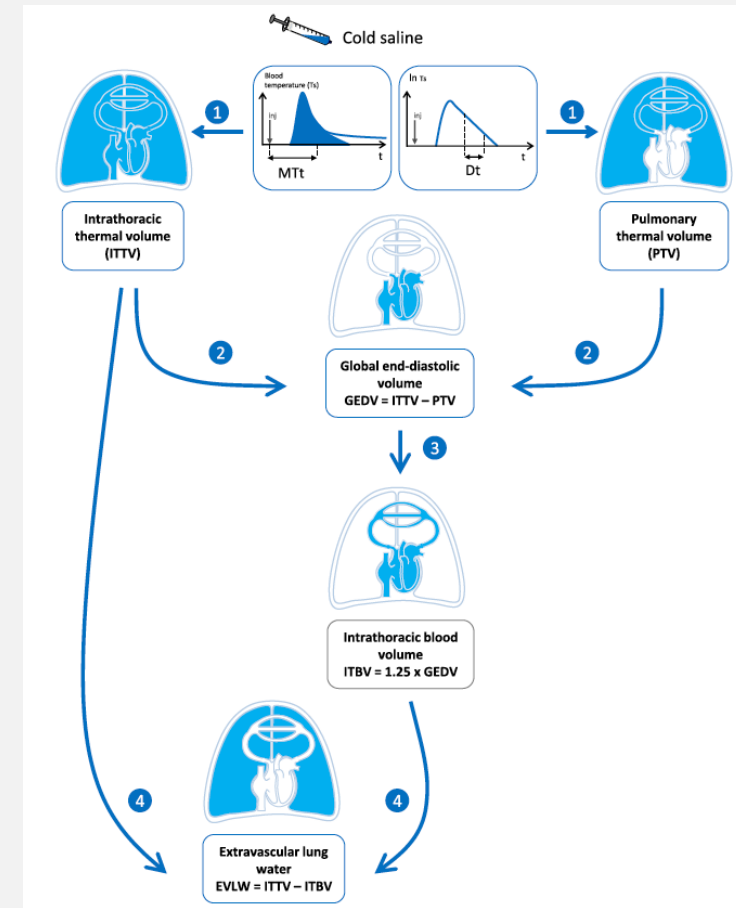
Area under the thermodilution curve



The CO is calculated from the area under the thermodilution curve^{18, 20}

TRANSPULMONARY THERMODILUTION

- TPTD also estimates some **intrathoracic volumes** base on analysis of the thermodilution curve and its logarithmic transformation
- According to Stewart Hamilton principle, total distribution volume of cold indicator between injection and detection sites represents the intrathoracic thermal volume
- Specific volumes
 - Intrathoracic thermal volume: $CO \times \text{mean transit time of cold indicator}$
 - Pulmonary thermal volume: $CO \times \text{downslope time of curve}$
 - Global end-diastolic volume: Intrathoracic thermal volume – total pulmonary volume; corresponds to volume of all 4 chambers at end of diastole (marker of preload)
 - Extravascular lung water: Intrathoracic thermal volume – intrathoracic blood volume ($ITBV = GEDV \times 1.25$)
 - Pulmonary vascular permeability index: $EVLW/\text{Pulmonary blood volume}$ (i.e. ratio of volume out of vessels to in vessels)



TRANSPULMONARY THERMODILUTION

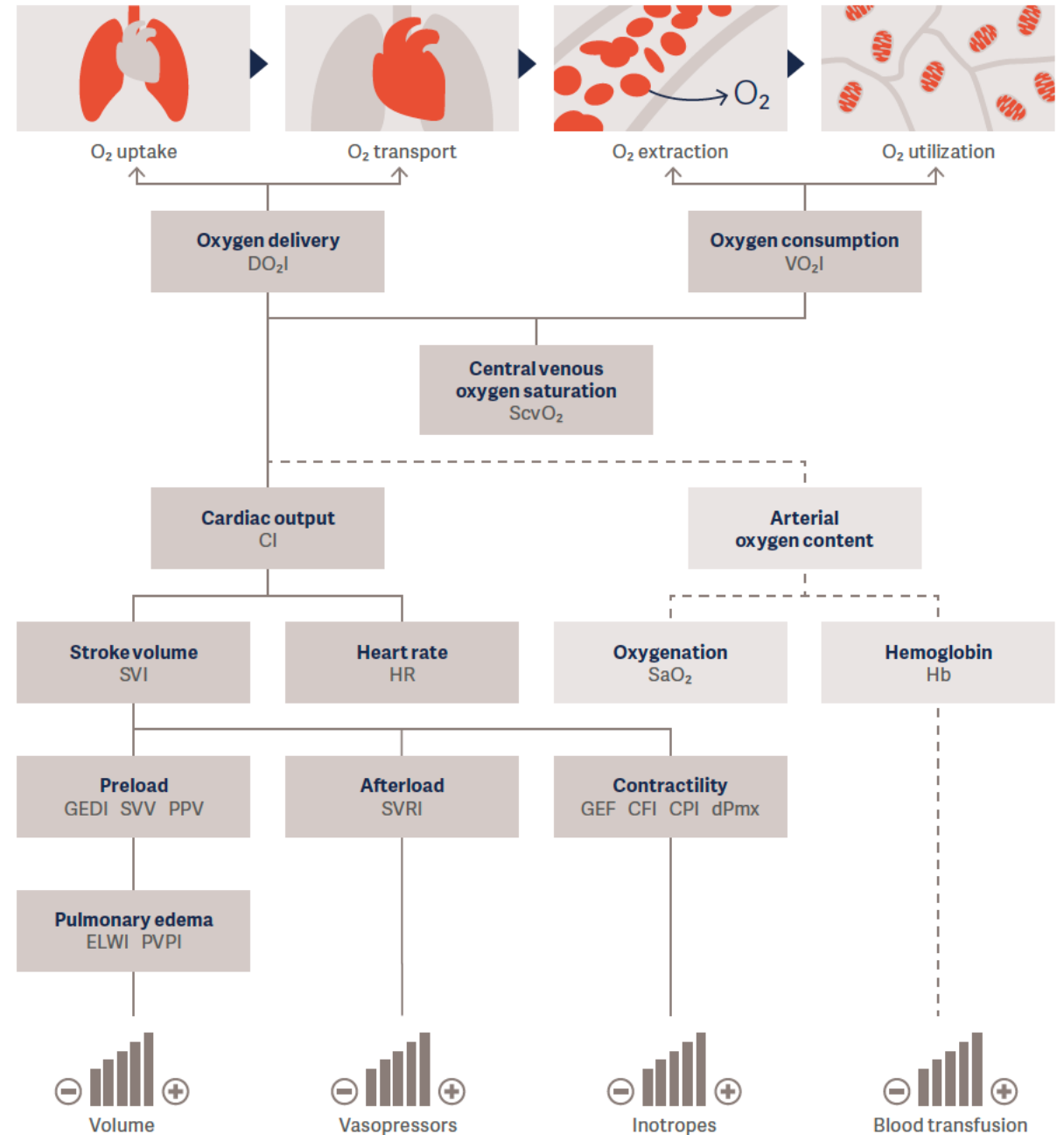
Variable	Clinical Significance	Normal Values	Limitations
Global end-diastolic volume	Preload	680-800ml/m ²	Does not distinguish between right and left ventricles, hence less directly reflects risk of pulmonary edema than PAOP
Cardiac function index, global ejection fraction	Cardiac contractility	CFI aim > 5, <2.3 suggests LVEF < 30% GEF 25-35%	Overestimates LV systolic function in case of RV dilation
Cardiac index	Affected by preload and contractility	Generally aim >2.2-2.5, but must contextualise to patient	
Extravascular lung water index	Marker of lung edema	3-7ml/kg (<10)	Unreliable in pulmonary embolism, lung resection, large pleural effusion
Pulmonary vascular permeability index	Discriminate between hydrostatic vs permeability	<3 cardiogenic edema, >3 permeability edema	Unreliable in pulmonary embolism, lung resection, large pleural effusion
Systemic vascular resistance index ((MAP-CVP)/CI) x 80	Afterload	1700-2400 dynes s m ² /cm ⁵	

Some caveats

- Femoral vein CVC: **Cannot be on same side as arterial catheter**. If on different side, cardiac output measurements still valid but **thoracic volumes invalid**
- Can be used in CRRT but not ECMO
- Can be used in therapeutic hypothermia
- Contraindicated in case of femoral vascular prosthesis (or other vascular related concerns)
- Unreliability in low CO states

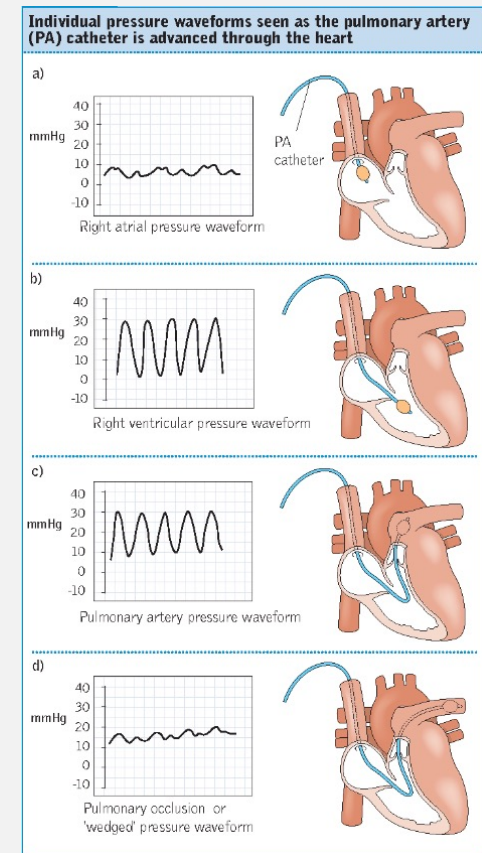
Clinical use

- May be particularly useful in ARDS with shock
- Thoracic volume indices may help with fluid management and de-resuscitation
- Measurement of cardiac output more robust than less invasive methods
- Incorporation of pulse contour analysis allows for real time and precise monitoring
- Unable to differentiate between right and left heart pathologies



PULMONARY ARTERY CATHETER

- Pulmonary artery catheters (PACs) are largely considered the gold standard for cardiac output monitoring because of accurate measurement method (thermodilution) and provision of right and left heart indices
- The catheter is inserted via a large vein into the RA > RV > PA. Catheter tip is intermittently wedged with an occlusion balloon in a tapering branch of the PA and a wedge pressure is obtained. Thermodilution is performed for cardiac output measurement.
- Main drawback is relative invasiveness and requirement for technical and interpretational expertise
- PACs are most useful in the context of right heart/biventricular cardiac dysfunction or pulmonary hypertension



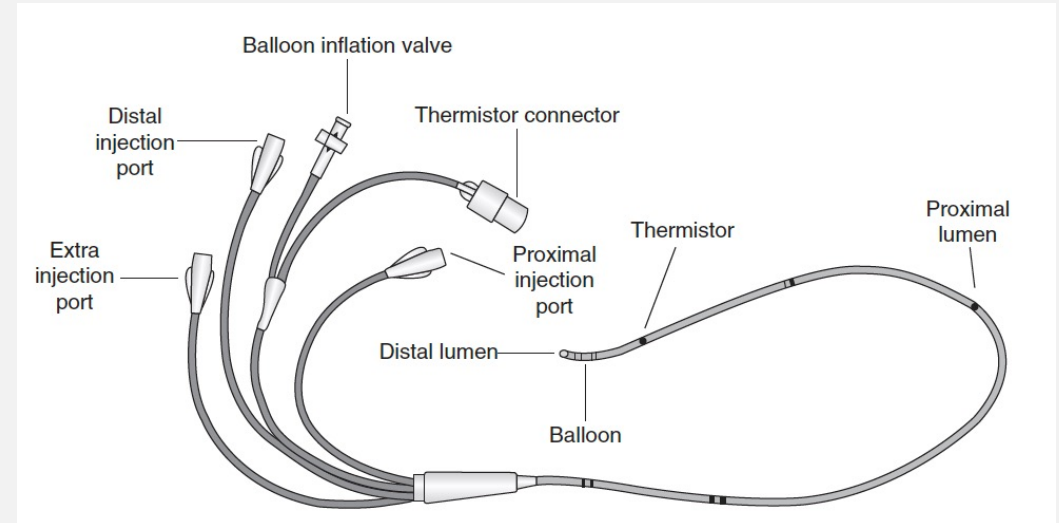
PULMONARY ARTERY CATHETER

- Measurements

- During insertion: RAP (1-6mmHg), RVP (15-30/1-6mmHg), PAP (15-30/6-12mmHg), PAWP (6-12mmHg)
- When in-situ: CO (thermodilution), PCWP (balloon occlusion), RAP, SvO₂ (available on some catheters)
- Calculated variables: PVR, SVR, SV, CPO, PAPi

- Clinical significance

- Preload: Right side (RAP), left side (PAWP)
- Contractility: CO, SV; these indices also affected by preload
- Afterload: Right side (PVRI 120-200), left side (SVRI 1700-2400)
- Oxygen supply-demand balance: SvO₂

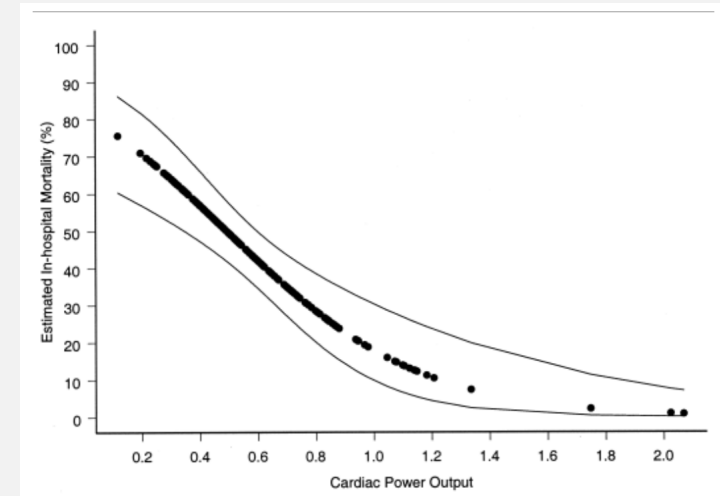


PULMONARY ARTERY CATHETER

	PCWP	CVP	CI	SVR	PVR
Hypovolemic	↓	↓	↓	↑	
Distributive	↓	↓	↑	↓	
Cardiogenic (RV)	-	↑	↓		↑
Cardiogenic (LV)	↑		↓	↑	
Cardiogenic (bivent)	↑	↑	↓	↑	
Tamponade	↑	CVP=PCWP		↑	

PULMONARY ARTERY CATHETER

- Cardiac power output
 - $[(\text{MAP} - \text{RAP}) \times \text{CO}] / 451$
 - Prognostic marker in cardiogenic shock - $<0.53\text{W}$ associated with 58% mortality
- Pulmonary artery pulsatility index (PAPi)
 - $(\text{PASP} - \text{PADP}) / \text{RAP}$
 - <1.5 associated with RV failure, <0.9 associated with severe RV failure



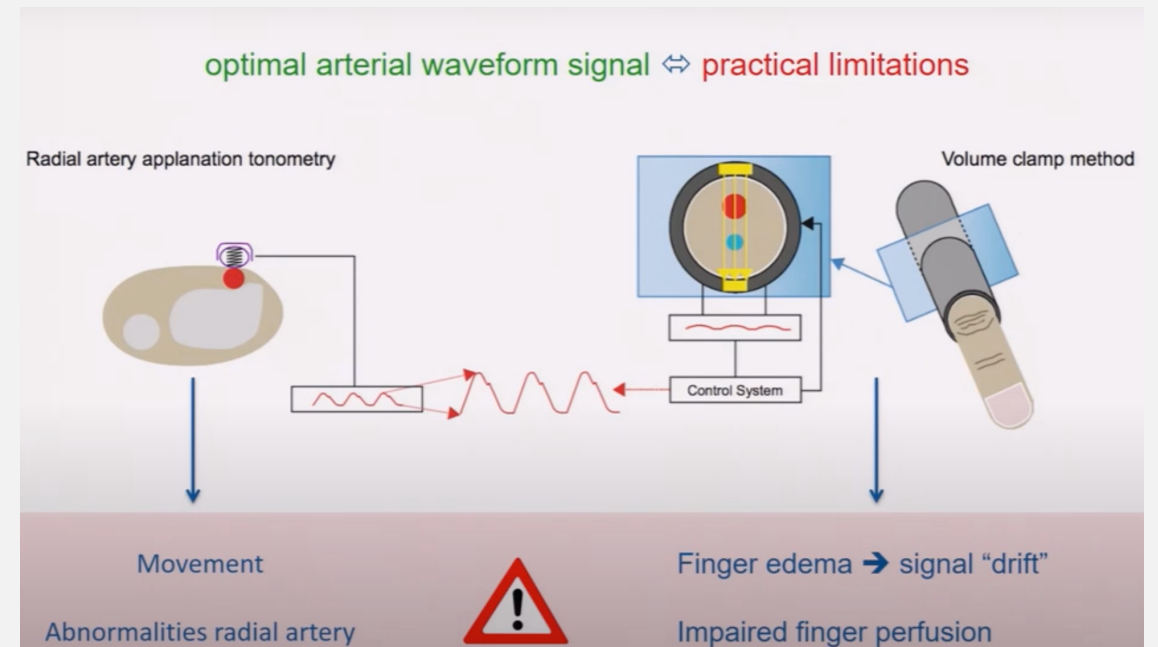
NON-INVASIVE PULSE CONTOUR ANALYSIS

Radial Artery Applanation Tonometry

- Electrico-mechanical sensor records arterial waveform over the radial artery – pulse contour analysis performed
- Limitations: Affected by sensor placement and movement

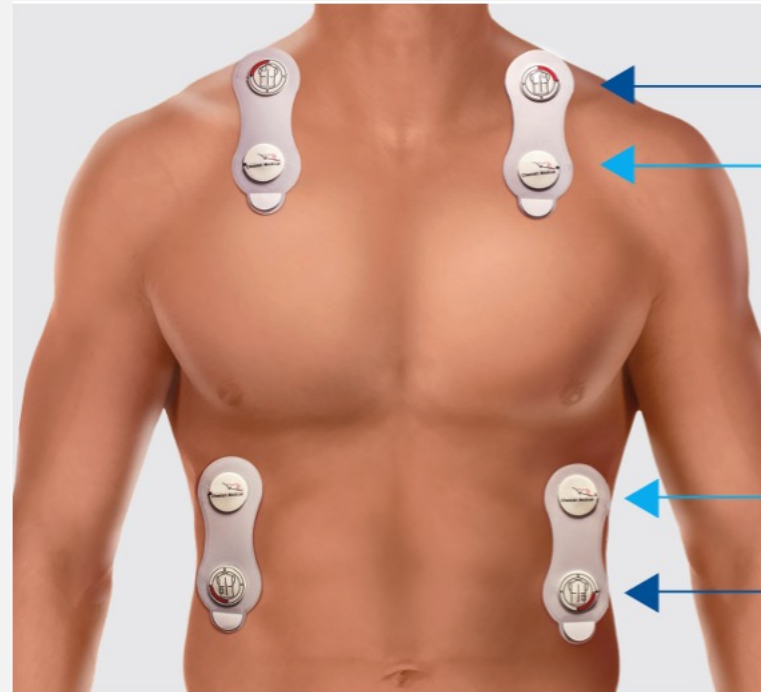
Volume Clamp Method

- Finger arterial pressure waveform derived from pressure needed to keep blood volume in finger artery constant – pulse contour analysis performed
- Limitations: May cause edema and vasoconstriction



BIOREACTANCE

- Stroke volume derived from phase shifts in voltage over the cardiac cycle because of pulsatile changes in intrathoracic blood volume
- Example: Baxter Starling device
- Stroke volume allows derivation of cardiac output and peripheral vascular resistance
- Can be used to monitor change in SV and CO following passive leg raise or fluid bolus
- Caution in pleural effusions, pulmonary edema, pacemaker, electrical interference, movement



Four non-invasive sensor pads are applied to the thorax, creating a "box" around the heart.

A small electric current is applied across the thorax between the outer pair of sensors.

A voltage signal is recorded between the inner pair of sensors.

The flow of blood in the thorax introduces a time delay or phase shift in the signal.

The monitor uses this phase shift as a baseline for stroke volume measurements.

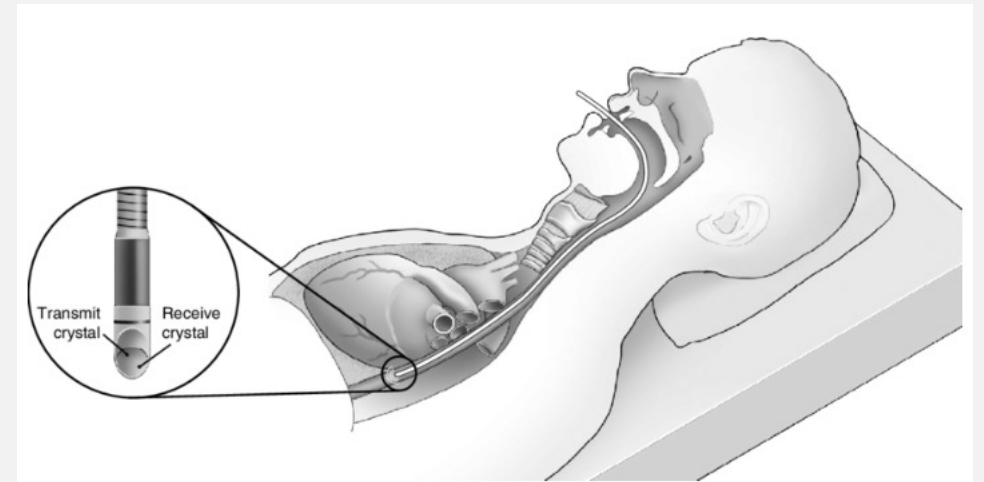
These signal changes have been correlated to known thermodilution cardiac output in 65,000 patient samples, in multiple clinical settings (ICU/OR/Cath Lab).^{9,13}

Baxter Starling brochure



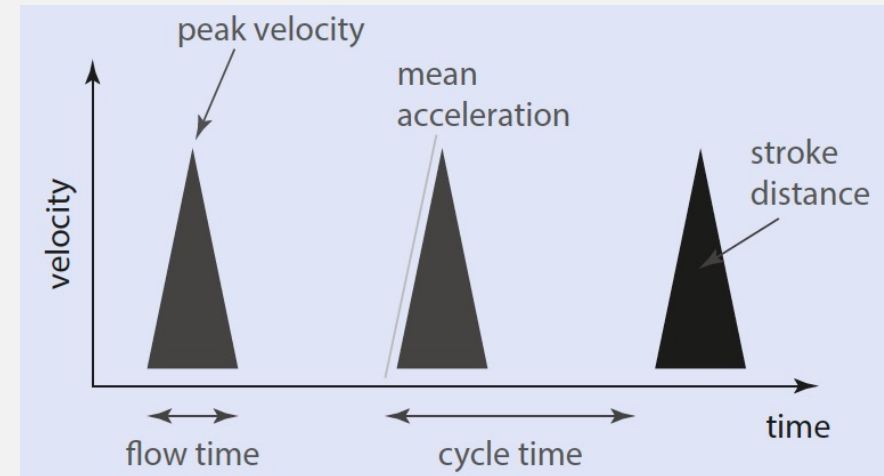
ESOPHAGEAL DOPPLER

- Doppler probe inserted into the midthoracic esophagus and is oriented posteriorly towards the descending aorta
- Continuous wave doppler is transmitted from the probe and a velocity time waveform is plotted based on reflected waves from red blood cells in aorta
- Limitations: SV derived base on nomogram, aortic cross-sectional area not measured, assumption of fixed distribution of cardiac output to descending aorta, positional dependence, assumption of lamina blood flow



ESOPHAGEAL DOPPLER

- **Stroke distance (SD)** is the area under the velocity-time waveform and represents distance moved by the column of blood within the aorta following left ventricular contraction. It is used to generate a nomogram-derived stroke volume, from which cardiac output ($HR \times SV$) can be derived.
- **Flow time (FT)** is the width of the base of the waveform and represents duration of systolic blood flow. The corrected flow time (FTc) which is adjusted for heart rate has a normal range of 330-360ms and is inversely related to vascular resistance. FTc is low in vasoconstricted states (e.g. hypovolemia) while FTc is high in vasoplegic states (e.g. sepsis)
- **Peak velocity (PV)** and mean acceleration (MA) are markers of left ventricular contractility – Normal range in 20yo (90-120cm/s), 70yo (50-70cm/s)



SUMMARY

- Simple shock: Monitoring with invasive blood pressure, ultrasound, biochemical markers (lactate, urine output)
- Mixed shock (mild): Consider monitoring ScvO₂, CO₂ gap, possible role for arterial line pulse contour analysis (but be aware of limitations)
- Severe/complex mixed shock or cardiogenic shock
 - Concomitant respiratory failure: Transpulmonary thermodilution
 - Cardiogenic shock: Consider PA catheter especially when component of RV dysfunction present, planning for MCS